

Original Article

Evaluating Denoising Using Various Techniques Based on Peak Signal-to-Noise Ratio and Mean-Square Error on CT Dental Images

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Abstract - In the field of clinical imaging, processed tomography (CT) is a critical instrument that analyzes the inward structures of a patient and gives precise clinical analysis. In this test, the portion of the radiation is legitimately connected with the nature of the picture procured. That is, a high radiation portion gives an excellent picture. Be that as it may, presenting patients to high dosages of radiation is hindering their wellbeing. In this way, to forestall the patient to consistent radiation introductions, the clinical network has been concentrating on diminishing the portion of radiation applied in CT checks. In this paper, we propose a special and nuclear method for the expulsion of Gaussian commotion from an uproarious advanced picture which isn't just fit for identifying and wiping out Gaussian clamour, present in the computerized picture yet in addition fit for creating an upgraded yield picture. We additionally attempt to set up that our proposed technique is giving a much better outcome in contrast with other well-known channels or calculations. To do that, we have conjured a similar report in trial results and examination part of these papers by figuring PSNR, MSE and MAE.

Keywords - PSNR, MSE, MAE, CT

I. INTRODUCTION

Innovation, for example, topographical data frameworks and cosmology. In a portion of the cases, every single pixel of the picture is indispensable, and if using any and all means a portion of the part of the picture is lost or noised, then it turns out to thoroughly esteem less. Clamour speaks to undesirable data which falls apart picture quality. Commotion is an arbitrary variety of picture forces. The commotion can be clarified as pixels inside the image present diverse force

esteems as opposed to addressing pixel esteems. The starting point of commotion can be from the physical nature of identification forms and has numerous particular structures and causes. It very well may be said that clamour is a procedure that influences the picture acquired and isn't a piece of the scene.

Commotion in the advanced picture may originate from different sources. The procurement procedure for computerized pictures changes over visible signs into electrical signals and afterwards into advanced signs is one procedure by which the clamour is presented in automated pictures. The above transformation process encounters vacillations, and every one of these means increases the value of the subsequent force of a given pixel.

A. Some sources of Noise are:

- When the image is scanned from a photograph made on film, here Noise can be produced from the damaged film or from the scanner used to take the image.
- If the image is taken directly in a digital format, the mechanism for gathering the data can introduce Noise.
- Insufficient light is also a cause of Noise due to which sensor temperature may introduce the Noise.
- Scratches and dust particles present in the scanner screen is also a cause of creating Noise.



B. Gaussian Noise

It is sure that each imaging strategy inalienably includes commotion. Numerous dabs can be seen in a photograph of a picture taken with an advanced camera because of low lighting conditions or the machine equipment issue. This sort of clamour is the uniform Gaussian commotion. Gaussian commotion is equitably circulated over the sign. This implies every pixel in the loud picture is the whole of the genuine pixel esteem and an irregular Gaussian dispersed commotion esteem. Gaussian clamour is otherwise called Amplifier commotion.

C. Salt and Pepper Noise

Noise: On the loss of gathering or recovering any pictures from the capacity gadget, arbitrary high contrast snow like examples can be seen on the pictures. This sort of commotion is called Salt and Pepper clamour. Salt and pepper clamour is a motivation sort of commotion, which is additionally alluded to as power spikes. This is caused commonly because of blunders in information transmission. A picture containing Salt and Pepper commotion will have dim pixels in splendid locales and the other way around.

D. Speckle Noise

Dot commotion can be demonstrated by arbitrary qualities increased by pixel esteems, so it is known as multiplicative clamour—spot clamour influences all sound imaging frameworks, including clinical ultrasound. The commotion usually taints clinical pictures in its procurement and Transmission. The presence of Speckle Noise influences the undertakings of individual translation and conclusion. Dot commotion is a significant issue in some Radar applications. Spot clamour is essentially present in Ultrasound pictures, Satellite pictures.

E. Poisson Noise

Poisson Noise is the Noise that is caused when a number of photons sensed by the sensor are not sufficient to provide detectable statistical information. This Noise exists because a phenomenon such as light and electric current consists of the movement of discrete packets. Poisson Noise may be dominated when the finite number of particles that carry energy is sufficiently small so that uncertainties due to the Poisson distribution, which describe the occurrence of independent random events, are of significance. The

magnitude of Poisson noise increases with the average magnitude of the current or intensity of the light.

F. Filter Used

a) Wallis Filter

The Wallis Filter process (Interpret/Raster/Filter/Wallis) applies a locally-versatile (spatially-differing) differentiate improvement to a grayscale raster. This channel is intended for grayscale pictures in which there are critical territories of brilliant and dull tones. An ordinary worldwide complexity improvement (e.g., Linear, Normalized) can't at the same time produce great neighbourhood differentiation at the two finishes of the splendour extend.

b) Edge Preserving Filter

Edge-safeguarding smoothing is a picture preparing method that smooths away commotion or surfaces while holding sharp edges. Models are the middle, reciprocal, guided, and anisotropic dissemination channels.

c) The Proposed Filter

In this part, propelled by the former examinations, we propose a versatile fourth-request picture denoising model. In this model, we attempted to explain the accompanying fourth-request limit esteem issue.

d) Butterworth Filter

In the field of Image Processing, Butterworth Filter is utilized for picture smoothing in the recurrence area. It expels high-recurrence clamour from a digital picture and jelly low-recurrence segments.

e) CT Dental Images

In the field of clinical imaging, registered tomography (CT) is a critical apparatus that inspects the inner structures of a patient and gives precise clinical analysis. In this test, the portion of the radiation is straightforwardly connected with the nature of the picture gained. That is, a high radiation portion gives an excellent picture. Be that as it may, presenting patients to high portions of radiation is hindering their wellbeing. Consequently, so as to forestall the patient to steady radiation presentations, the clinical network has been concentrating on lessening the portion of radiation applied in CT examines.

II. RESULTS AND DISCUSSION

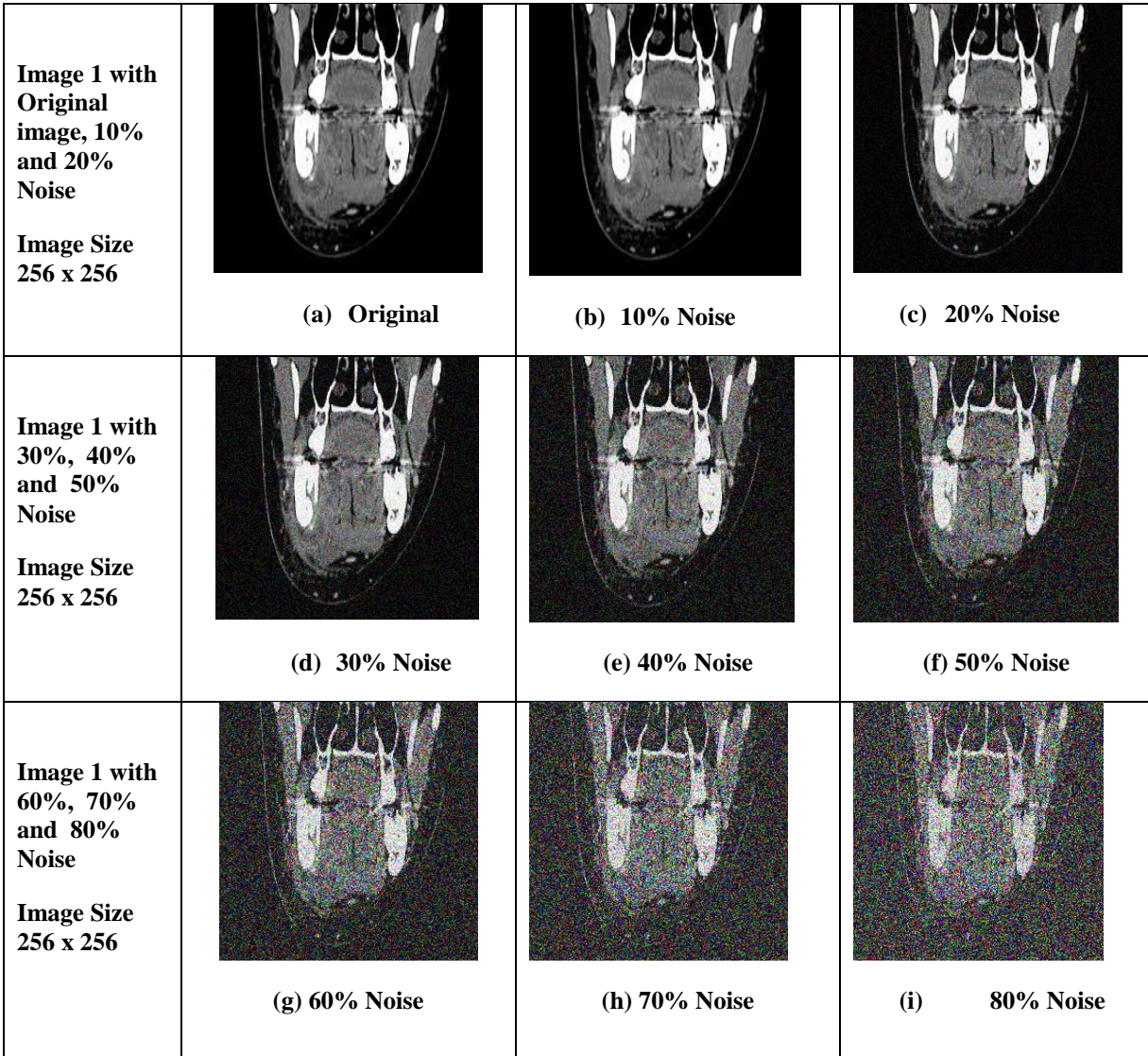


Fig. 1 Image 1, PSNR and MSE results achieved with different models, (256 x 256) on (a) Original image. (b) 10% Noisy image (c) 20% Noisy image (d) 30% Noisy image (e) 40% Noisy image (f) 50% Noisy image (g) 60 % Noisy image (h) 70% Noisy image (i) 80% Noisy image.

Table 1. Analysis for image1 containing 10% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	15.98	16.40	20.57
Edge Preserving	8.51	91.50	83.06
Proposed Filter	18.04	10.20	7.89
Butterworth Filter	7.85	106.47	86.69

Table 2. Analysis for image1 containing 20% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	14.41	23.54	30.53
Edge Preserving	8.15	88.64	81.94
Proposed Filter	16.11	15.91	13.01
Butterworth Filter	7.96	103.9	85.72

Table 3. Analysis for image1 containing 30% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	14.26	24.34	31.61
Edge Preserving	8.78	85.93	80.88
Proposed Filter	15.46	18.46	15.19
Butterworth Filter	8.07	101.31	84.83

Table 4. Analysis for image1 containing 40% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	14.05	25.57	32.93
Edge Preserving	8.89	83.94	80.15
Proposed Filter	14.71	21.98	18.36
Butterworth Filter	8.16	99.24	84.28

Table 5. Analysis for image1 containing 50% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	13.81	27.01	34.55
Edge Preserving	8.93	83.10	79.95
Proposed Filter	14.01	25.81	21.86
Butterworth Filter	8.20	98.27	84.33

Table 6. Analysis for image1 containing 60% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	13.46	29.28	36.42
Edge Preserving	8.91	84.43	80.25
Proposed Filter	13.58	28.45	23.96
Butterworth Filter	8.21	97.97	84.66

Table 7. Analysis for image1 containing 70% Noise Intensity

Name of the Filter	PSNR	MSE	MAE
Walis Adaptive Filter	13.05	32.2	38.48
Edge Preserving	8.87	84.29	80.88
Proposed Filter	12.91	33.21	27.42
Butterworth Filter	8.21	98.02	85.15

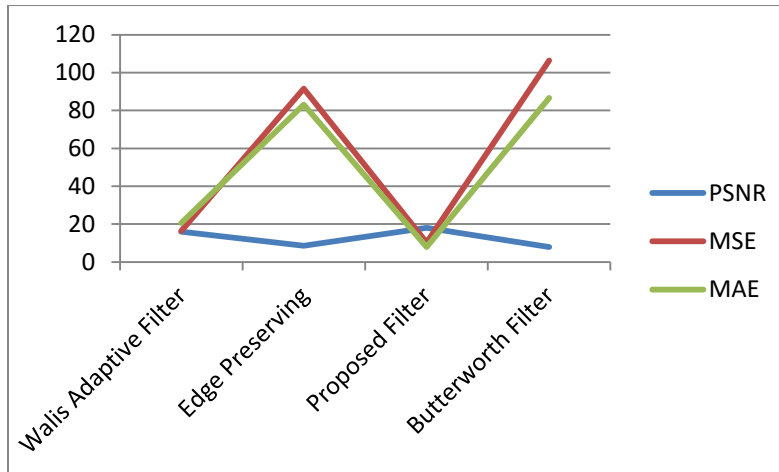


Fig. 2 Performance of different filters on an image1 having 10% noise intensity

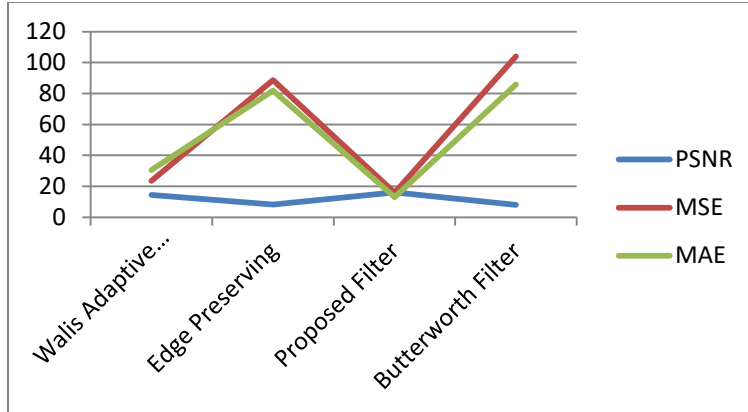


Fig. 3 Performance of different filters on an image1 having 20% noise intensity

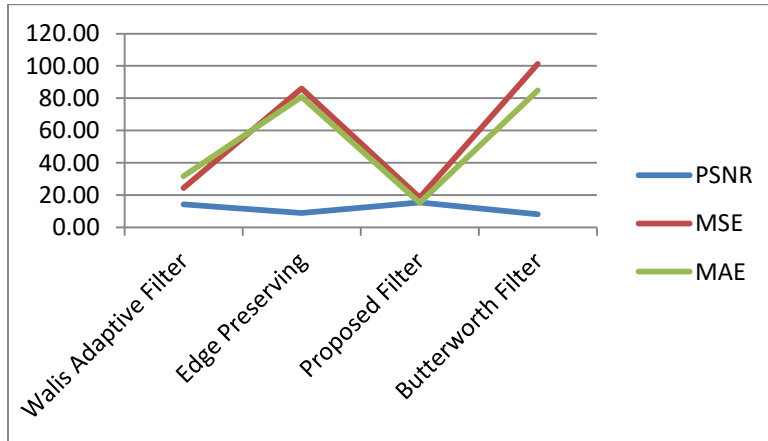


Fig. 4 Performance of different filters on an image1 having 30% noise intensity

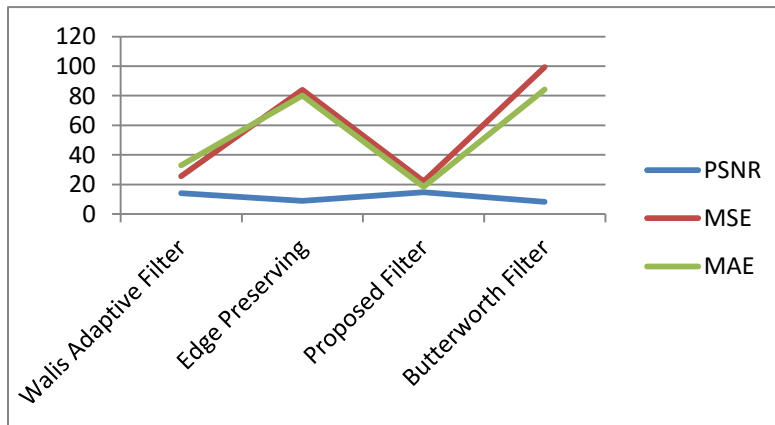


Fig. 5 Performance of different filters on an image1 having 40% noise intensity

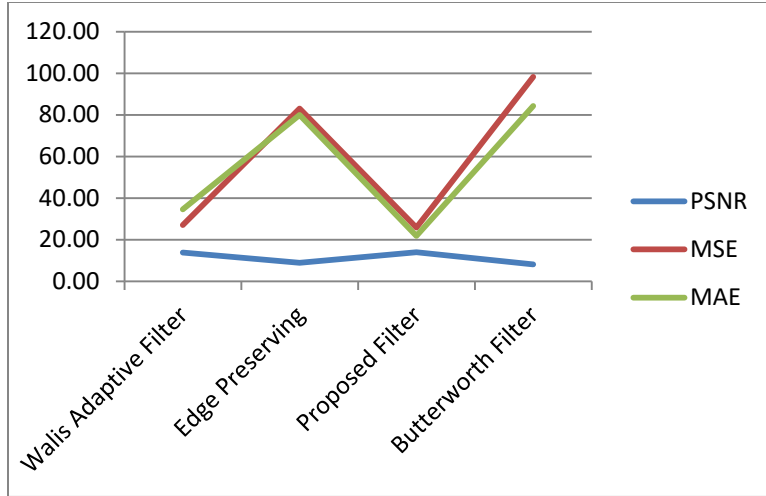


Fig. 6 Performance of different filters on an image1 having 50% noise intensity

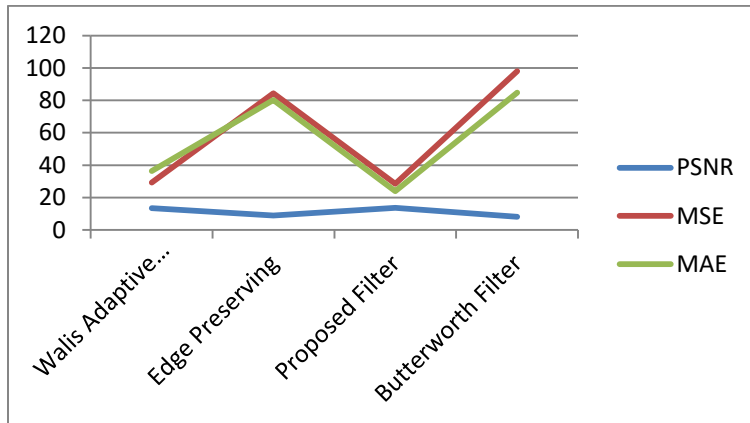


Fig. 7 Performance of different filters on an image1 having 60% noise intensity

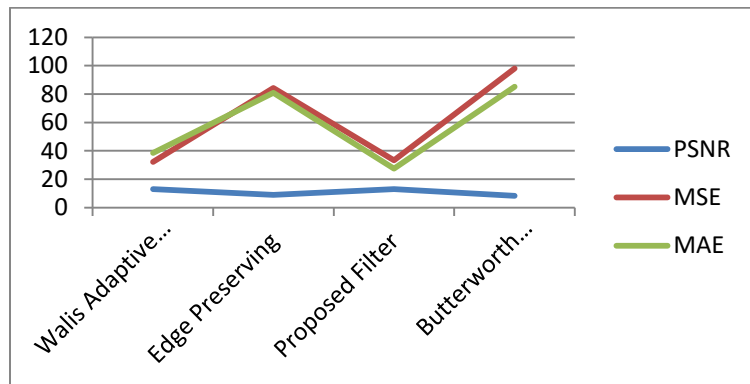


Fig. 8 Performance of different filters on an image1 having 70% noise intensity

III. CONCLUSION

For biomedical applications like CT dental analysis and segmentation, Image preprocessing is necessary to be done on images to get accurate segmented results. Analysis of various techniques of image preprocessing, which includes resizing, grey level conversion, histogram enhancement process, is performed. Correctly, image noise plays a vital role in image processing. Applied proposed and various other filters to the input image and its PSNR, MSE and MAE values are determined, which shows that Proposed Filter shows better performance in PSNR, MSE and MAE of the output image. Table 5.1 to 21 and Fig. 5.10 to 5.37 get the results from a reconstructed image with high PSNR, low MSE and MAE values.

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